

Mixtures of Gaussian Wells: Theory, Computation, and Application in Immunofluorescence Histology

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Abstract

A primary challenge in unsupervised clustering using mixture models is the selection of a family of basis distributions flexible enough to succinctly represent the distributions of the target subpopulations. In this paper we introduce a new family of Gaussian Well distributions (GWDs) for clustering applications where the target subpopulations are characterized by hollow [hyper-]elliptical structures. We develop the primary theory pertaining to the GWD, including mixtures of GWDs, selection of prior distributions, and computationally efficient inference strategies using Markov chain Monte Carlo. We demonstrate the utility of our approach, as compared to standard Gaussian mixture methods, for the case of immunofluorescence imaging analysis, emphasizing the improved interpretability and parsimony of the GWD-based model.

Keywords: Gaussian mixtures, Poisson point processes, subtractive mixtures, histology

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1. Introduction

Bayesian nonparametric mixture modeling, as exemplified by the Dirichlet process mixture model (DPM) (Müller and Quintana, 2004), has emerged as a standard statistical technique for flexible density estimation and model-based clustering. Much of the appeal of this approach stems from two features of the inference process. First, in contrast to traditional finite mixture models, the DPM specifies a mixture model with infinite component capacity, thus eliminating the requirement that the user specify *a priori* the number of mixture components. Second, the standard data augmentation scheme for performing inference on a mixture model involves the estimation of latent parameters that associate observations with individual components in the mixture model. These indicator variables can be regarded to indicate cluster membership, and as such the DPM has gained popularity as a probabilistic clustering technique.

The success of the DPM as a clustering technique, however, lies in the ability of the mixture model components to efficiently represent the probability distributions of the subpopulations of observations that constitute the individual “clusters”. For example, the multivariate Gaussian DPM is often employed for clustering applications involving observations with continuous valued features. In such cases, it is often necessary for the practitioner to perform manual annotation of the inferred mixture components in order to reconcile occurrences of multiple mixture components jointly characterizing individual “clusters.”

In this paper, we introduce a new family of Gaussian Well Distributions (GWDs) for use in spatial clustering applications where the aim is to identify hollow regions characterized by density “wells”. The Gaussian

27 well components of such a model are themselves *subtractive* mixtures of two
28 multivariate Gaussian distributions. Existing approaches have focused on
29 modelling hollow structures by fitting the data onto the surface of a hyper-
30 ellipse or torus (Mardia and El-Atoum, 1976; Kato, 2010; Di Marzio et al.,
31 2011; Kanatani and Rangarajan, 2011; Jones and Pewsey, 2011; Umbach
32 and Jones, 2003; Watson, 1961; Gander et al., 1994), which can be too re-
33 strictive and does not offer an accurate representation of many other types
34 of circular data. In contrast, the Gaussian well distribution provides pos-
35 itive probability density throughout the \mathbb{R}^p space, except for singularities;
36 the mode of this distribution subsequently corresponds to a hyper-ellipse.

37 Our motivation stems from the analysis of immunofluorescence imaging
38 data. Immunofluorescence imaging provides measurements of the intensities
39 of cellular surface proteins tagged with fluorescent markers. This technique
40 is often applied to tissue samples, in order to characterize the tissue com-
41 position in terms of the spatiotemporal distributions of distinct cell types
42 as identified by their unique surface proteins. A fundamental goal of this
43 type of analysis is the unsupervised identification of the emergence of cel-
44 lular structures called *germinal centers*, which are formed as part of the
45 organism’s immune response to some stimulus (Figure 1).

46 Following Kottas and Sansó (2007), who proposed the use of the Dirich-
47 let process as a random mixing distribution of bivariate Beta distributions to
48 model spatial point processes, Ji et al. (2009) recently demonstrated a novel
49 computational approach for analyzing data of this type by characterizing the
50 incidence of each pixel’s fluorescence level for a particular tagged protein as
51 a realization of a spatially inhomogeneous Poisson process. The intensity
52 function of the Poisson process was modelled using a Dirichlet process mix-
53 ture of bivariate Gaussian distributions, thus enabling the representation

54 of arbitrarily complex spatial arrangements of the marked cells. However,
55 representation of the intensity function as an additive mixture of Gaussian
56 kernels only allowed identification of the germinal centers by manual in-
57 spection and annotation due to the inability of the Gaussian components
58 to succinctly represent the density “wells” that characterize the germinal
59 centers.

60 Here we extend the approach of these authors by modelling the inten-
61 sity function of the spatially inhomogeneous Poisson process as a mixture of
62 Gaussian well distributions. We demonstrate that in addition to providing
63 greater interpretability, our approach is more parsimonious and computa-
64 tionally efficient, requiring fewer mixture components and therefore fewer
65 model parameters.

66 The remainder of the paper is organized as follows. Section 2 provides
67 the basic definition and properties of the Gaussian well distribution and mix-
68 tures thereof. Section 3 provides details on selection of prior distributions
69 and develops a computationally efficient inference strategy via MCMC. Sec-
70 tion 4 discusses the application of a Gaussian well modeling approach to the
71 analysis of immunofluorescence imaging data obtained from a vaccine design
72 experiment. Section 5 concludes with a discussion of alternative applications
73 and future work.

74 **2. The Gaussian Well Distribution**

75 *2.1. Basic theory*

76 In this section we develop the basic theory for the Gaussian Well Dis-
77 tribution (GWD). We begin by defining the GWD, in its basic form, as a
78 subtractive, rather than an additive, mixture of two multivariate Gaussian

79 kernels:

80 **Definition 1.** *Given non-negative scalars w and v and p -dimensional Gaus-*
 81 *sian kernels $N(\mu_1, \Sigma_1)$ and $N(\mu_2, \Sigma_2)$, a Gaussian Well Distribution is a*
 82 *multivariate continuous probability distribution characterized by the density*
 83 *function $f : \mathbb{R}^p \rightarrow \mathbb{R}_0^+$ such that*

- 84 1. $f(x) = wN(x; \mu_1, \Sigma_1) - vN(x; \mu_2, \Sigma_2)$
- 85 2. $\forall x \in \mathbb{R}^p, f(x) \geq 0$
- 86 3. $\int f(x)dx = 1$

87 For appropriately chosen parameters, f resembles the Gaussian distribution
 88 $N(\mu_1, \Sigma_1)$ with a region of low density (i.e. a density “well”) with shape
 89 Σ_2 surrounding μ_2 . Figure 2 contains sample density surfaces for several
 90 GWDs in one and two dimensions.

91 The primary theory pertaining to the GWD has to do with defining the
 92 necessary constraints on the free parameters $w, v, \mu_1, \mu_2, \Sigma_1,$ and Σ_2 so
 93 that requirements 2 and 3 above hold. We begin with the following Lemma:

Lemma 1. *The parameters $w, v, \mu_1, \mu_2, \Sigma_1,$ and Σ_2 are valid for a Gaus-*
sian Well distribution (i.e. the positivity and integrability requirements will
be met) if and only if $v = w - 1$, and all eigenvalues of D are non-negative,
where

$$D = \left(\begin{array}{c|c} (-\Sigma_1^{-1} + \Sigma_2^{-1})/2 & 0.5 \times (\Sigma_1^{-1}\mu_1 - \Sigma_2^{-1}\mu_2) \\ \hline 0.5 \times (\mu_1'\Sigma_1^{-1} - \mu_2'\Sigma_2^{-1}) & 0.5 \times (\mu_2'\mu_2 - \mu_1'\mu_1) + \log\left(\frac{w}{w-1}\sqrt{\frac{|\Sigma_2|}{|\Sigma_1|}}\right) \end{array} \right),$$

94 where μ' denotes the vector transpose.

95 Proof that these constraints satisfy the positivity and integrability re-
 96 quirements appears in Appendix A.

97 From Lemma 1, we can immediately derive the following corollary.

98 **Corollary 2.** *In the special case $\mu_1 = \mu_2$, $\Sigma_2 = \tau\Sigma_1$, the positivity con-*
 99 *straint implies $\frac{w-1}{w} \leq \tau^{p/2} \leq 1$.*

100 Proof of the corollary appears in Appendix B. For this subclass of
 101 GWDs, the mode of the distribution is defined by an ellipsoid with equation

$$(x - \mu)' \Sigma^{-1} (x - \mu) = \frac{2\tau \log\left(\frac{w-1}{w} \tau^{-p/2-1}\right)}{1 - \tau},$$

revealing the relationship between the shape of the well and the parameters of the distribution. The shape of this distribution is therefore natural for discovering the ring-shaped germinal centers in our immunofluorescence application. In the special case $\frac{w-1}{w} = \tau^{p/2}$, corresponding to a subclass of GWDs which we will refer to as *Ring GWDs*, the equation becomes

$$(x - \mu)' \Sigma^{-1} (x - \mu) = \frac{2\tau}{\tau - 1} \log \tau.$$

102 In the remainder of paper, we focus on the special case where $\mu_1 =$
 103 $\mu_2 := \mu$ and $\Sigma_2 = \tau\Sigma_1 := \tau\Sigma$. This form of the distribution is used below
 104 in deriving a representation of mixtures of GWDs.

105 2.2. Mixtures of Gaussian Wells

We define a mixture of the special class of ring GWDs ($\mu_2 = \mu_1$ and $\Sigma_2 = \tau\Sigma_1$) as a convex combination of Ring GWD components

$$f(x|\boldsymbol{\pi}, \boldsymbol{w}, \boldsymbol{\mu}, \boldsymbol{\Sigma}, \boldsymbol{\tau}) = \sum_{k=1}^K \pi_k f_k(x|w_k, \mu_k, \Sigma_k, \tau_k),$$

where

$$f_k(x|w_k, \mu_k, \Sigma_k, \tau_k) = w_k N(x|\mu_k, \Sigma_k) - (w_k - 1)N(x|\mu_k, \tau_k \Sigma_k),$$

106 and $\{\boldsymbol{\pi}, \mathbf{w}, \boldsymbol{\mu}, \boldsymbol{\Sigma}, \boldsymbol{\tau}\}$ denotes the set of parameters for all components.

107 The mixture representation can be simplified using ring GWD, which
 108 have density exactly 0 at $x = \mu$, occurring when $\tau = \left(\frac{w_k-1}{w_k}\right)^{2/p}$. This leads
 109 to the following lemma:

Lemma 3. *Any ring GWD*

$$f(x|w, \mu, \Sigma) = wN(x|\mu, \Sigma) - (w - 1)N(x|\mu, \tau\Sigma)$$

can be re-written as

$$f(x) = \tilde{\pi}_1 g_1(x) + \tilde{\pi}_2 g_2(x),$$

110 where $g_1(x)$ is a ring GWD and $g_2(x)$ is a standard [multivariate] Gaussian
 111 kernel.

112 Proof of the Lemma appears in Appendix C.

This result implies that the class of mixture models with ring GWD components is a subset of the class of mixture models with components either ring GWDs or standard Gaussian densities. Thus, we will be able to perform inference on the ring GWD mixture model by considering a more general mixture model capable of representing both ring GWD components and standard Gaussian components. Thus, our target mixture model is defined by

$$f(x) = \sum_{k=1}^K \pi_k f_k(x),$$

113 where each component has the following distribution

$$f_k(x) = \begin{cases} N(x|\mu_k, \Sigma_k) & \text{w.p. } (1 - \rho), \\ w_k N(x|\mu_k, \Sigma_k) - (w_k - 1)N\left(x\left|\mu_k, \left(\frac{w_k - 1}{w_k}\right)^{2/p} \Sigma_k\right.\right) & \text{w.p. } \rho, \end{cases}$$

Here ρ is the marginal probability of any individual mixture component being a ring GWD component (as opposed to a standard Gaussian component). Since a standard Gaussian component can be viewed as a Gaussian well component with $a_k = 1$, we can express our mixture model using only Gaussian well components, so that

$$f(x) = \sum_{k=1}^K \pi_k w_k N(x|\mu_k, \Sigma_k) - (w_k - 1)N\left(x\left|\mu_k, \left(\frac{w_k - 1}{w_k}\right)^{2/p} \Sigma_k\right.\right),$$

114 such that $w_k = 1$ with probability $1 - \rho$ corresponds to (with a slight abuse
115 of notation) the limiting case of a standard Gaussian kernel.

116 3. Prior Distributions and Posterior Inference

117 Having defined the GWD mixture model in the previous section, we now
118 motivate prior distributions for its parameters and describe a Markov chain
119 Monte Carlo algorithm for conducting inference.

120 3.1. Priors for component mixing weights π

121 We use a standard truncated Dirichlet process prior for the mixing
122 weights π using a concentration parameter $\alpha \sim Ga(\nu_\alpha, \lambda_\alpha)$. Denoting the
123 latent component configuration indicators as z_i , for each observation x_i we
124 have $z_i|\pi \sim \text{Multinomial}(\pi, 1)$ (see Ishwaran and James, 2002). The mixing

125 weights π therefore follow the standard form for the stick-breaking repre-
 126 sentation of a Dirichlet process mixture model:

$$\begin{aligned} \pi_k | V_1, \dots, V_k &= V_k \prod_{j=1}^{k-1} (1 - V_j) \text{ for } k = 1 \dots K \\ V_j | \alpha &\sim \text{Beta}(1, \alpha) \text{ for } k = 1 \dots K - 1 \\ V_K &= 1. \end{aligned}$$

127 *3.2. Priors for subtractive mixture weights $\{w_k\}$*

128 As mentioned above, the subtractive mixture weight w_k is exactly 1 with
 129 probability $1 - \rho$, and takes values in $(1, \infty)$ otherwise. The choice of prior on
 130 the subtractive mixture weights $w_k \in (1, \infty)$ determines the expected shape
 131 of the Gaussian well components. Different values of w_k lead to a variety of
 132 differently shaped wells. For example, in one dimension, with $w_k > 1$, the
 133 width of the Gaussian well increases with w (Figure 3).

134 In order to obtain further intuition about the behaviour of w , we observe
 135 that any distribution $f(x|\theta) = w f_1(x|\theta) - (w - 1) f_2(x|\theta)$, $w > 1$, which
 136 satisfies $f(x|\theta) \geq 0 \quad \forall x$, can be realized through the following rejection
 137 sampler:.

- 138 1. Draw a random variable from distribution $f_1(x)$.
- 139 2. Accept that value with probability $1 - \frac{(w-1)f_2(x)}{w f_1(x)}$.
- 140 3. The accepted values will have distribution $f(x)$.
- 141 4. The rejected values will have distribution $f_2(x)$.

In the case of $f(x) = w N(x|\mu, \Sigma) - (w - 1) N(x|\mu, \tau \Sigma)$, given the data X
 and the parameters μ and Σ , we have exact forms for the envelope dis-
 tribution $f_1(x) = N(x|\mu, \Sigma)$ and the distribution of the rejected values

$f_2(x) = N(x|\mu, \tau\Sigma)$. This implies that generating values for $Y \sim f_2(x)$ and combining them with the data X , the set $\{X, Y\}$ should be well modelled by $f_1(x)$. The information about w does not come from the shape of the rejected sample, but rather from the *number of rejected observations*, n_2 , required to produce $n = |X|$ accepted samples from the target distribution. According to the rejection sampling mechanism, for each accepted observation correspond $\frac{w}{w-1}$ rejected ones. In other words, the number of total observations drawn from $f_1(x)$ to obtain n accepted values is negative binomially distributed with probability $\frac{w-1}{w}$. We therefore use a natural re-parametrization in which we express w through the probability $\tau := \frac{w-1}{w} \in (0, 1)$, resulting in a Beta prior

$$\tau_k = \frac{w_k - 1}{w_k} \sim Be(p_1, p_2)$$

142 with probability ρ , and $\tau_k = 0$ with probability $1 - \rho$.

143 3.3. Priors on component-specific parameters $\{\mu_k, \Sigma_k\}$

144 We denote the means and variances of the Gaussian wells by (μ_k, Σ_k) .
 145 The conjugate prior for $\{\mu_k, \Sigma_k\}|\{\tau_k = 0\}$ is a Normal-Inverse Wishart
 146 distribution such that $\Sigma_k|\{\tau_k = 0\} \sim IW(d, S)$ and $\mu_k|\{\tau_k = 0, \Sigma_k\} \sim$
 147 $N(0, t_0\Sigma_k)$. In the case of the Gaussian wells, we use $\Sigma_k|\{\tau_k > 0\} \sim$
 148 $IW(d^\dagger, S^\dagger)$ and $\mu_k|\{\tau_k > 0, \Sigma_k\} \sim N(0, t_0^\dagger\Sigma_k)$

149 Standard conjugacy results hold for the standard Gaussian components.
 150 In the case of the GWD components, this leads to posteriors of non-standard
 151 forms, for which Metropolis steps are required. Details on posterior approx-
 152 imation are provided in the next section.

153 *3.4. Markov chain Monte Carlo sampler*

154 We now describe a Markov chain Monte Carlo algorithm for produc-
 155 ing samples from the joint posterior distribution $p(\alpha, \mu, \Sigma, \tau, \pi|X)$. A key
 156 novelty of our approach lies in the use of Gibbs and Metropolis-Hastings up-
 157 dates based on tractable approximations for the true posterior distributions
 158 of the parameters. This ensures rapid mixing and convergence to the target
 159 stationary distribution of the Markov chain. The algorithm is as follows:

- 160 1. Update τ_k by proposing $\tau_k = 0$ with probability ρ and $\tau_k \sim U(0, 1)$ oth-
 161 erwise, accepting/rejecting according to the corresponding Metropolis-
 162 Hastings ratio.
- 163 2. The means and covariances μ_k and Σ_k of components with $\tau_k = 0$ can
 164 be updated through Gibbs steps.
3. The means of the GWDs can be updates through a variance-discounted
 version of the standard Gaussian - inverse Wishart form, such that

$$q(\mu_k | \{X, z, \tau_k > 0, \Sigma_k\}) = N\left(\frac{\bar{x}_k n_k t_0^\dagger}{1 + n_k t_0^\dagger}, 4 \frac{t_0^\dagger \Sigma_k}{1 + n_k t_0^\dagger}\right),$$

165 where \bar{x}_k represents the sample mean of component k and n_k the
 166 number of observations in component k . The proposed values are
 167 then accepted/rejected according to the Metropolis-Hastings ratio.

- 168 4. In order to approximate the posterior distribution of Σ_k for GWDs,
 169 we use the fact that

$$\text{Var}(x_{z_i=k}) = w_k \times \Sigma_k - (w_k - 1) \times \tau_k \Sigma_k$$

which provides an estimate for the posterior mean of Σ_k . Using the
 factor $c_k = w_k + (1 - w_k)\tau_k = w_k + (1 - w_k) \left(\frac{w_k - 1}{w_k}\right)^{2/p}$, we use the fol-

lowing distribution in order to approximate the posterior distribution,
so that

$$q(\Sigma_k | \{X, z, \tau_k > 0\}) = IW \left(d^\dagger + n_k, S^\dagger + \sum_{z_i=k} (x_i - \bar{x}_k)(x_i - \bar{x}_k)' / c_k \right),$$

170 where, as before, \bar{x}_k denotes the sample mean of component k and
171 n_k the number of observations in component k . The proposed values
172 are then accepted/rejected according to the corresponding Metropolis-
173 Hastings ratio.

174 5. Finally, standard Gibbs steps are used for the updates of α , π and z
175 (see Ishwaran and James, 2002).

176 4. Application in immunofluorescence histology

177 The motivating application for this work arises in immunological stud-
178 ies in mice where multiple images provide data on the spatial configuration
179 of many immune cells in a specific, localized region of lymphatic or spleen
180 tissues. A single experiment views an image as the response to stimulus
181 via injection of a vaccine, the overall context being exploration of responses
182 under candidate vaccine designs. Observed measurements are fluorescent
183 intensities generated from tagged cell-surface proteins that characterize a
184 specific cell type. Interest lies in characterizing the spatial intensity func-
185 tions underlying observed data in each image, and feeding the statistical
186 summaries and characterizations into visual and numerical comparisons.

187 Following Ji et al. (2009), our general statistical framework jointly mod-
188 els the fluorescence intensity function of the signal as a spatially inhom-
189 geneous Poisson process and the noisy outcome of the point process; see

190 Appendix for details. Here we use mixtures of both Gaussian wells and
 191 standard Gaussian components, providing a better representation of ger-
 192 minal centre structure using fewer components. The Markov chain Monte
 193 Carlo sampler described in Section 3.4 is integrated within the algorithm
 194 presented in Ji et al. (2009).

195 We implement our algorithm on images of size $n_1 \times n_2$. The axes are
 196 transformed so that the x and y ranges are both $[-5, 5]$ by dividing them
 197 by K_x and K_y respectively, and centering. We assume priors for the image
 198 and noise signals:

$$\begin{aligned} (m_y|v, y) &\sim N(m_y|\bar{m}_y, tv_y) \\ v_y^{-1} &\sim Ga(c_v/2, c_v/(2\bar{v}_y)). \end{aligned}$$

199 Here $m_0 = 3.75$, $m_1 = 4.5$, $t = 0.05$, $\bar{v}_0 = 0.25$, $\bar{v}_1 = 0.5$ and $c_v = 10$.

200 4.1. Fitting a single Gaussian well structure

201 We implement our algorithm on a zoomed-in image of simply one germi-
 202 nal centre shown in Figure 4 (a), where a single Gaussian well-like structure
 203 is identifiable by eye. We use the following priors for signal and background,
 204 and intensity function of the occupied pixels through the Gaussian well mix-
 205 ture. As described in Section 3.1, we use a mixture model where each com-
 206 ponent is either a GWD or a standard Gaussian distribution, with prior
 207 probability of each $\rho = 0.5$. For the prior of the Dirichlet concentration
 208 parameter $\alpha \sim Ga(10^{-4}, 10^{-4})$. The prior of the covariance matrices of the
 209 outside well is given by $\Sigma_k|\{\tau_k > 0\} \sim IW(10, 100I)$, whereas the covariance
 210 matrices of the standard Gaussian components $\Sigma_k|\{\tau_k = 0\} \sim IW(10, 10I)$.
 211 The means of the GWDs and standard Gaussians are given by $\mu_k|\{\tau_k >$

212 $0, \Sigma_k\} \sim N(0, 5\Sigma_k)$ and $\mu_k|\{\tau_k = 0, \Sigma_k\} \sim N(0, 5\Sigma_k)$ respectively. We place
 213 a Beta prior on $\tau_k = (w_k - 1)/w_k \sim Be(10, 1)$. We run the sampler for 2000
 214 iterations fixing the maximum number of components at 15, discarding the
 215 first 1000 as burn-in.

216 As is shown in Figure 4 (b) and (c), the data are fitted well by a single
 217 Gaussian well component, with some additional structure represented by
 218 an extra standard Gaussian component with very low weight; the posterior
 219 intensity surface shows an accurate representation of the original image.

220 4.2. Fitting full image: B220 PA alone day 26

221 Finally, we fit our algorithms to the whole image shown in Figure 5
 222 (a). In this case there are several regions with Gaussian well shape, most
 223 of which represent germinal centre follicles, but also several regions with
 224 standard Gaussian shape. Owing to the flexibility of the model, the image
 225 is fitted by several standard and well Gaussians. We use a Gamma prior
 226 of the Dirichlet concentration parameter $\alpha \sim Ga(10^{-4}, 10^{-4})$. The prior
 227 of the covariance matrices of the outside well is given by $\Sigma_k|\{\tau_k > 0\} \sim$
 228 $IW(100, 10I)$, whereas the covariance matrices of the standard Gaussian
 229 components $\Sigma_k|\{\tau_k = 0\} \sim IW(5, 0.5I)$. The increased degrees of freedom
 230 in the Inverse Wishart prior distribution of the Gaussian Wells allow us to
 231 strongly incorporate expert knowledge about the shape and size of germinal
 232 centre follicles, as opposed to spurious well-like structures. The means of the
 233 GWDs and standard Gaussians are given by $\mu_k|\{\tau_k > 0, \Sigma_k\} \sim N(0, 10\Sigma_k)$
 234 and $\mu_k|\{\tau_k = 0, \Sigma_k\} \sim N(0, 30\Sigma_k)$ respectively, and we place a Beta prior
 235 on $\tau_k = (w_k - 1)/w_k \sim Be(10, 1)$. We run the sampler for 2000 iterations
 236 fixing the maximum number of components at 15, discarding the first 1000
 237 as burn-in.

238 Figure 5 (b) and (c) show that our sampler identifies around 10 Gaussian
239 well components, which successfully correspond to germinal centre follicle
240 candidates identifiable by eye. Comparison against the posterior distribution
241 samples obtained using a standard Gaussian mixture model in Figure 6
242 shows a significant improvement both in the ability to identify these follicles,
243 but also in terms of an accurate representation of the original image.

244 5. Discussion

245 We have presented a new class of Gaussian mixture distributions which
246 allow for negative mixing weights, resulting in probability density functions
247 which resemble hollow volumes; in the case of 2 dimensions, these structures
248 look like wells. Our flexible mixture modeling approach can simultaneously
249 model highly unstructured inhomogeneous regions through a very flexible
250 prior and germinal centre follicles with a distinct hollow structure with a
251 more informative prior using experts' knowledge about the shape and struc-
252 tures of the germinal centres. Our approach allows us to identify candidate
253 germinal centres; these can then be used to subsequently compute mea-
254 sures like average and total intensity within each Gaussian well, in order to
255 characterize and compare germinal centres within and across images.

256 Although we have only implemented our methods on immunofluorescence
257 histology datasets, our models can be applied to a variety of other applied
258 fields, such as medical imaging, astronomy or synthetic biology, where data
259 are often dispersed around, but not restricted to, an ellipse, a sphere or a
260 circle.

261 Natural extensions to our methods include investigating the properties
262 and devising priors that allow for asymmetric Gaussian well distributions.

Figure 1: A single germinal center of a mouse lymph node stained for B220 cells.

Figure 2: Examples of Gaussian Well distributions in 1 and 2 dimensions. The left-hand column shows “ring wells” in 1 and 2 dimensions, in which the density is exactly 0 at the centre of the well. The rightmost column shows Gaussian wells with equal means; in the top row, the variances are chosen such that the the center of the well has strictly positive density, and the bottom row demonstrates the effect of asymmetric covariance matrices.

263 While providing a much more general class of distributions, constructing
264 efficient proposals for exploring the sample space is crucial.

265 Our Markov chain Monte Carlo sampler was implemented in MATLAB;
266 code is available upon request.

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Figure 3: Probability density functions for 1-dimensional ring GWDs using $\mu_1 = \mu_2 = 0$ and $\sigma_1 = 1$ for increasing values of w .

276 References

277 Di Marzio, M., Panzera, A., Taylor, C.C., 2011. Kernel density estimation
278 on the torus. *Journal of Statistical Planning and Inference* 141, 2156 –
279 2173.

Figure 4: A single germinal centre zoomed in. The leftmost figure shows the original images, representing a zoomed-in version of the lymph node of a mouse stained for B220. The middle figure shows the component structure at a single iteration of the MCMC, and rightmost figure shows the posterior mean intensity function. The Gaussian well successfully shapes around the germinal centre structure using a single Gaussian well component and an additional standard Gaussian component in order to account for the slight asymmetry of the germinal centre.

Figure 5: The full image, on the left, of a B220 stain from a mouse lymph node. The middle figure shows the component structure at a single iteration of the MCMC, and the right one shows the posterior mean intensity function. The Gaussian well structures model the 6/7 germinal centres visibly identifiable in the original image, with more than one component required for some.

- 280 Gander, W., Gander, W., G, W., Golub, G.H., Strebler, R., 1994. Fitting of
281 Circles and Ellipses - Least Squares Solution. Technical Report. ETH.
- 282 Ishwaran, H., James, L., 2002. Approximate Dirichlet process computing
283 in finite normal mixtures: Smoothing and prior information. *Journal of*
284 *Computational and Graphical Statistics* 11, 508–532.
- 285 Ji, C., Merl, D., Kepler, T., West, M., 2009. Spatial mixture modelling for
286 unobserved point processes: Examples in immunofluorescence histology.
287 *Bayesian Analysis* 4, 297–316.
- 288 Jones, M.C., Pewsey, A., 2011. Inverse batschelet distributions for circular
289 data. *Biometrics* , no–no.
- 290 Kanatani, K., Rangarajan, P., 2011. Hyper least squares fitting of circles
291 and ellipses. *Computational Statistics and Data Analysis* 55, 2197 – 2208.
- 292 Kato, S., 2010. A markov process for circular data. *Journal of the Royal*
293 *Statistical Society: Series B (Statistical Methodology)* 72, 655–672.
- 294 Kottas, A., Sansó, B., 2007. Bayesian mixture modeling for spatial poisson

Figure 6: Mixture structure and intensity plot for the same image using a standard Gaussian mixture model.

- 295 process intensities, with applications to extreme value analysis. *Journal*
296 *of statistical planning and inference* 137, 3151–3163.
- 297 Mardia, K.V., El-Atoum, S.A.M., 1976. Bayesian inference for the von
298 mises-fisher distribution. *Biometrika* 63, 203–206.
- 299 Müller, P., Quintana, F., 2004. Nonparametric Bayesian data analysis. *Sta-*
300 *tistical Science* 19, 95–110.
- 301 Umbach, D., Jones, K.N., 2003. A few methods for fitting circles to data.
302 *IEEE Transactions on Instrumentation and Measurement* 52.
- 303 Watson, G.S., 1961. Goodness-of-fit tests on a circle. *Biometrika* 48.

304 **Appendix A. Proof of Lemma 1**

Lemma. *The parameters $w, v, \mu_1, \mu_2, \Sigma_1,$ and Σ_2 are valid for a Gaussian Well distribution (i.e. the positivity and integrability requirements will be met) if and only if $v = w - 1,$ and all eigenvalues of D are non-negative, where*

$$D = \left(\begin{array}{c|c} (-\Sigma_1^{-1} + \Sigma_2^{-1})/2 & 0.5 \times (\Sigma_1^{-1}\mu_1 - \Sigma_2^{-1}\mu_2) \\ \hline 0.5 \times (\mu_1'\Sigma_1^{-1} - \mu_2'\Sigma_2^{-1}) & 0.5 \times (\mu_2'\mu_2 - \mu_1'\mu_1) + \log\left(\frac{w}{w-1}\sqrt{\frac{|\Sigma_2|}{|\Sigma_1|}}\right) \end{array} \right),$$

305 where μ' denotes the vector transpose.

306 *Proof.* The function requirement trivially integrates to 1 iff $v = w - 1.$

307 The positivity requirement $f(x) = wf_1(x) - vf_2(x) \geq 0$ is equivalent to

308 $\log(wf_1(x)) - \log(vf_2(x)) \geq 0.$ Then we have

$$\begin{aligned} \log(f_1(x)) - \log(f_2(x)) &= \log(w) - 0.5 \log(2\pi|\Sigma_1|) - \frac{1}{2}(x - \mu_1)'\Sigma_1^{-1}(x - \mu_1) \\ &\quad - \log(1 - w) + 0.5 \log(2\pi|\Sigma_2|) + \frac{1}{2}(x - \mu_2)'\Sigma_2^{-1}(x - \mu_2) \\ &= \log\left(\frac{w}{v}\sqrt{\frac{|\Sigma_2|}{|\Sigma_1|}}\right) - \frac{1}{2}(x - \mu_1)'\Sigma_1^{-1}(x - \mu_1) + \frac{1}{2}(x - \mu_2)'\Sigma_2^{-1}(x - \mu_2) \end{aligned}$$

309 which can be written as a quadratic form

$$(x_1 \cdots x_p \ 1)D(x_1 \cdots x_p \ 1)'$$

310 where

$$D = \left(\begin{array}{c|c} (-\Sigma_1^{-1} + \Sigma_2^{-1})/2 & 0.5 \times (\Sigma_1^{-1}\mu_1 - \Sigma_2^{-1}\mu_2) \\ \hline 0.5 \times (\mu_1'\Sigma_1^{-1} - \mu_2'\Sigma_2^{-1}) & 0.5 (\mu_2'\mu_2 - \mu_1'\mu_1) + \log\left(\frac{w}{v}\sqrt{\frac{|\Sigma_2|}{|\Sigma_1|}}\right) \end{array} \right)$$

311 In the above symmetric matrix $D,$ the left upper-triangular $p \times p$ matrix is

312 equal to $(\Sigma_1^{-1} - \Sigma_2^{-1})/2$, the first p entries of the $p+1$ column of the matrix
 313 are equal to $\Sigma_1^{-1}\mu_1 - \Sigma_2^{-1}\mu_2$, and the $(p+1, p+1)$ entry of the matrix is
 314 equal to $-0.5\mu'_1\mu_1 + 0.5\mu'_2\mu_2 + \log\left(\frac{w}{v}\sqrt{\frac{|\Sigma_2|}{|\Sigma_1|}}\right)$.

315 Thus the original inequality reduces to the requirement that D be posi-
 316 tive semi-definite, which will be true when all eigenvalues of D are positive.
 317 Thus it is necessary that $\Sigma_1^{-1} - \Sigma_2^{-1}$ is positive semi-definite, representing
 318 the intuitive condition that $f_2(x)$ must have lighter tails than $f_1(x)$. A fur-
 319 ther necessary condition is that all diagonal elements are positive, which in
 320 this case requires $-0.5\mu'_1\mu_1 + 0.5\mu'_2\mu_2 + \log\left(\frac{w}{v}\sqrt{\frac{|\Sigma_2|}{|\Sigma_1|}}\right) > 0$. \square

321 Appendix B. Proof of Corollary 2

322 **Corollary.** *In the special case $\mu_1 = \mu_2$, $\Sigma_2 = \tau\Sigma_1$, the positivity constraint*
 323 *implies $\frac{w-1}{w} \leq \tau^{p/2} \leq 1$.*

324 *Proof.* In the special case $\mu_1 = \mu_2$ and $\Sigma_2 = \tau\Sigma_1$, we have

$$D = \left(\begin{array}{c|c} (1 - 1/\tau)\Sigma_1^{-1}/2 & 0 \\ \hline 0 & \log\left(\frac{w}{v}\sqrt{\tau^p}\right) \end{array} \right)$$

325 This implies that, in order for D to be positive semi-definite, we require
 326 $\frac{w-1}{w} \leq \tau^{p/2} \leq 1$. \square

327 Appendix C. Proof of Lemma 3

Lemma. *Any ring GWD*

$$f(x|w, \mu, \Sigma) = wN(x|\mu, \Sigma) - (w-1)N(x|\mu, \tau\Sigma)$$

can be re-written as

$$f(x) = \tilde{\pi}_1 g_1(x) + \tilde{\pi}_2 g_2(x),$$

328 where $g_1(x)$ is a ring GWD and $g_2(x)$ is a standard [multivariate] Gaussian
 329 kernel.

Proof.

$$\begin{aligned} wN(\mu, \Sigma) - (w - 1)N(\mu, \tau\Sigma) = \\ \tilde{\pi}_1 \left(\frac{1}{1-\tau^{\frac{p}{2}}} N(\mu, \Sigma) - \left(\frac{1}{1-\tau^{\frac{p}{2}}} - 1 \right) N(\mu, \tau\Sigma) \right) + \tilde{\pi}_2 N(\mu, \tau\Sigma), \end{aligned}$$

330 where $\tilde{\pi}_1 = w(1 - \tau^{\frac{p}{2}})$, $\tilde{\pi}_2 = 1 - \tilde{\pi}_1$. □

331 **Appendix D. Indirectly observed point process**

332 Since the cells are much larger than each individual pixels, each pixel is
 333 assumed to be either occupied by a cell or is empty, corresponding to signal
 334 or noise in the model. Occupied pixels are modeled as an inhomogeneous
 335 Poisson process, with Poisson intensity surface of the signal following a ran-
 336 dom mixture of 2-dimensional Gaussian wells. In other words, the locations
 337 $\mathbf{x} = \{x_i\}$ of cells are independent 2-dimensional variates with probability
 338 density function of a mixture of Gaussian wells.

339 Using the de-composition into standard Gaussian and Gaussian Well
 340 components (see Section 3), the mixture model can be realized through a
 341 set of latent configuration indicators c_i for each observation x_i , allocating
 342 each observation to precisely one component of the mixture model (either
 343 Gaussian well or standard Gaussian), allowing to improve efficiency of the
 344 algorithms Ishwaran and James (2002). Here the number of components

345 is unknown, and we use flexible priors for their location, spread and well
 346 parameter $\theta_k = (w_k, \mu_k, \Sigma_k)$.

Following Ji et al. (2009), we define a latent binary indicator $y \in \{0, 1\}$, corresponding to the absence or presence, respectively, of cell-associated immunofluorescence in the pixel region with index point $x_i \in \mathcal{X}$. Then the likelihood function fits the set of observed points $\{x \in \mathcal{X} : y(x) = 1\}$, corresponding to pixels occupied by a part of a cell, such that

$$p(X|\gamma, f) \propto \exp(-\gamma)\gamma^N / a^{2N} \prod_{i=1}^N f(x_i).$$

347 Here γ represents the overall scale parameter $\gamma = \int_{x \in S} \lambda(x) dx$, S being
 348 the finite image region, and a^2 is the 2-dimensional pixel region. Given the
 349 binary probability indicator for each pixel, $p(z|y = 0, \mu)$ represents back-
 350 ground noise in the absence of an object at a specific location, and similarly
 351 $p(z|y = 1, \mu)$ represents noise in the presence of a signal. Then if $z = z(y(x))$
 352 represents measured fluorescence at pixel region x , the $p(z|y, \mu)$ is defined
 353 by

$$\begin{aligned} (\log(z)|y = 0) &\sim N(m_0, v_0)I(\log(z) < h_2), \\ (\log(z)|y = 1) &\sim N(m_1, v_1)I(h_1 < \log(z) < h_2), \end{aligned}$$

354 where m_0, v_0 relates to the background noise and (m_1, v_1) to signal fluores-
 355 cence. The upper truncation is inherent to the digital fluorescent image bit
 356 depth and the lower truncation h_1 of the image signal is introduced as an
 357 identifying criterion which distinguishes between signal and noise.